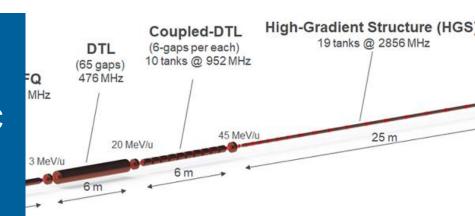
HIAT-2022 CONFERENCE DARMSTADT, GERMANY, JUNE 27 – JULY 1ST, 2022



DEVELOPMENTS TOWARDS A COMPACT CARBON ION LINAC FOR CANCER THERAPY



PRESENTER

Brahim Mustapha Physics Division Argonne National Laboratory



June 27th, 2022 HIAT Conference (via Zoom)

Content

- ☐ Accelerators in Ion Beam Therapy Why not a Linac?
- ☐ Overview of the Advanced Compact Carbon Ion Linac (ACCIL) Design

- ☐ Main Design Choices / Features of the ACCIL Linac
- ☐ Development of High-Gradient Structures for Ion Beams
- ☐ ACCIL Capabilities for Ion Beam Therapy and Other Applications
- ☐ Future Plans

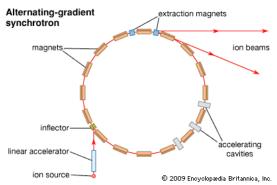
Accelerators in Ion Beam Therapy

✓ Cyclotrons for protons

Synchrotrons for carbon ions

Fixed-energy electromagnet cw machine (north pole) acceleration, particle's path hollow electrode chambers charged particle--target alternating current electromagnet source (south pole)

Variable energy Pulsed machine



✓ Why Not a Linac?

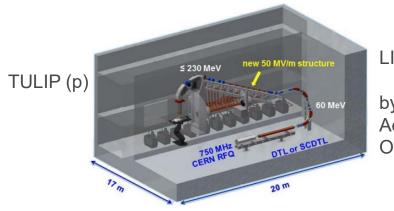
	Cyclotron	Synchrotron	Linac
Variable energy	With degrader	From pulse to pulse without losses	From pulse to pulse without losses
Beam quality	Bad quality due to energy degrader	Good	Better
Repetition rate	-	~ 1 Hz	~ 100 Hz

Why Not a Linac?

- Using the same technology used for high-intensity research machines, a 400 MeV/u carbon ion linac would be 100s meters long!
- BUT, we don't need a high-intensity machine, only 10¹⁰ particles/second
- Low intensity → Small aperture → High frequency → High voltage
- Low intensity → Short pulses → Low duty cycle → Even higher voltage
- For protons, carbon and other ions, it's possible to deliver the required beam intensity in ~ µs long pulses at ~ 100 Hz repetition rate
- We can take advantage and build on recent progress in high-frequency highgradient structure R&D for electrons

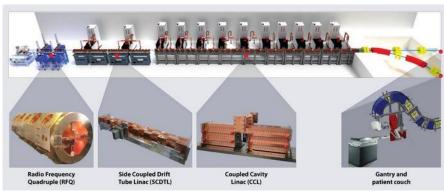
Linacs for Proton / Ion Therapy

- ✓ First proposal for a proton therapy linac: R. W. Hamm et al, "Preliminary Design of a Dedicated Proton Therapy Linac", Proceedings of PAC-91
- ✓ Recent developments in Europe → The LIGHT system is now operational in the UK



LIGHT (p)

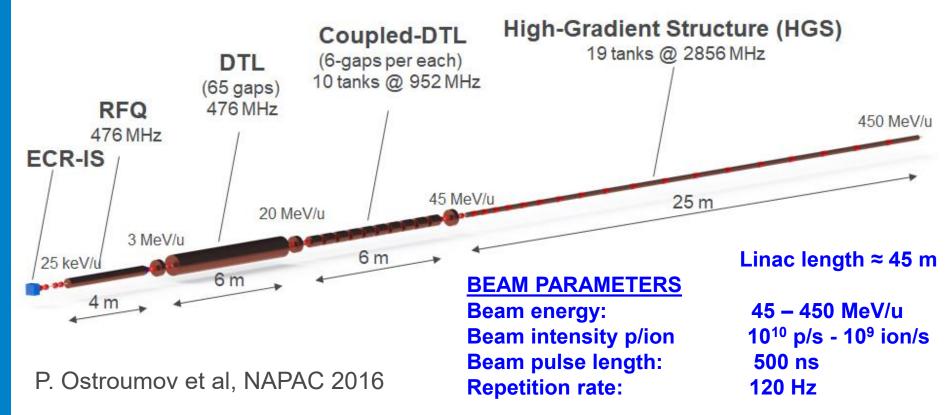
by Advanced Oncotherapy



Others: CABOTO (C), LIBO, IMPLART, PERLA,...

✓ Main parts of these accelerators operate at 3 GHz (S-band)

ACCIL: Advanced Compact Carbon Ion Linac



Key Component: High-Gradient Structures for Low-Velocity Ions

Developments towards ACCIL for Cancer Therapy







Main Design Features / Choices for ACCIL

- Required carbon beam intensities can be provided by commercial ECRs, a 5+ charge state for carbon beam is selected to avoid contaminants
- ✓ The acceleration starts with a 476 MHz RFQ designed for ¹²C⁵⁺
- ✓ Stripping to 6+ after RFQ, further acceleration by a DTL with PMQs designed to focus both proton and carbon beams without tuning
- ✓ Frequency transition and further acceleration and by a CCDTL at 972 MHz
- ✓ Transition to high-energy linac at 45 MeV/u, based on S-band accelerating structures (2856 MHz) using commercially available klystrons
- ✓ High accelerating gradients up to 50 MV/m in S-band structure are possible due to very short RF pulse, less than 1 μs Manageable voltage breakdown rate
- ✓ Short beam pulses are acceptable because the average current is very low
- ✓ High repetition rate of beam pulses, ~ 100 Hz or higher, is required for fast scanning of a tumor

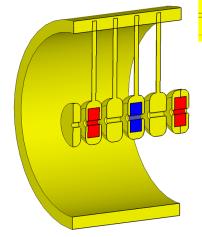


476 MHz RFQ and DTL – Design Parameters

	RFQ	DTL
lons	C ⁵⁺	C ₆₊
Energy in, MeV/u	0.025	-
Energy out, MeV/u	3	20
Length, m	4	5.82
Epeak, Kilpatrick units	2.6	2.0
Aperture radius, mm	2.0	5.0
Q_0	10 ⁴	5*10 ⁴
Intervane voltage, kV	80	-
Real estate acc. Gradient, MV/m	~1.0	3.5
P _{pulse} , MW	0.44	4.88

Brazed 352 MHz Linac4 RFQ segment (Courtesy of CERN)







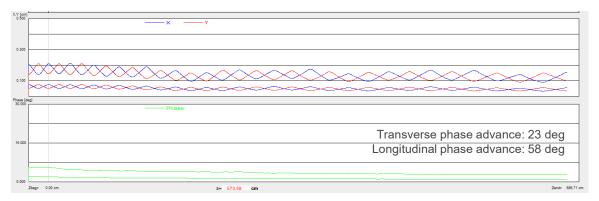
FODO lattice $L_f = 4\beta\lambda$

DTL with permanent magnet quadrupole focusing – non tunable

PMQ (140 T/m)

PMQ Focusing in DTL for Carbon & Proton

Carbon Beam in DTL



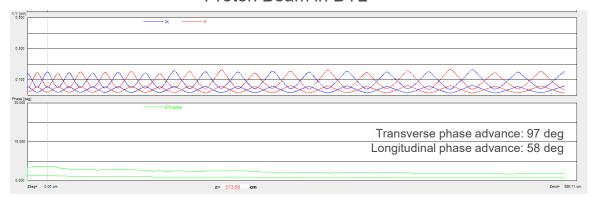
Non-tunable PMQs



Different transverse phase advances for proton and carbon

Accelerating rate is the same

Proton Beam in DTL



Developments towards ACCIL for Cancer Therapy

972 MHz Coupled Cavity DTL

Ions: Carbon (6+)

Energy Range: 20 - 45 MeV/u

Length: 0.37-0.54 m

Q: 35 000

RF Power: 12.7 MW

 $ZT^2 = 54 M\Omega/m$

Esmax: 2.05 Kilpatricks

2a = 1.0 cm

 $E_0 = 18-17 \text{ MV/m}$

 $E_0T = 12 \text{ MV/m}$

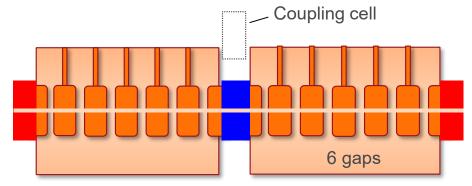
 $\phi_s = -24..-17 \text{ deg}$

 $3\tau = 52 \mu sec$

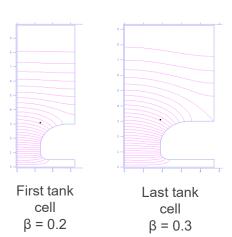
 Δ = 0.2% @ 120 Hz

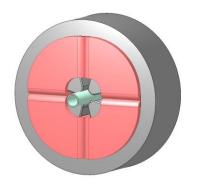
G = 90 T/m

 $L_q = 6.2 \text{ cm}$



10 tanks $L_f \approx (13-15)\beta\lambda$





Compact EMQ (90 T/m)

2856 MHz Coupled Cavity Linac (CCL)

Constant E0T = 50 MV/m along the whole high- β section (19 tanks)



Ions: Carbon (6+)

Energy Range: 45 – 450 MeV/u

Length: 0.32-1.4 m

Q: 7500..17000

RF Power: 1065 MW

 $ZT^2 = 19..57 M\Omega/m$

Esmax: 2.2-1.6 Kilpatricks

2a = 0.6 cm

 $E_0 = 67-70 \text{ MV/m}$

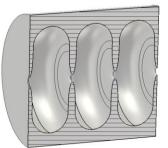
 $E_0T = 50 \text{ MV/m}$

 $\phi_s = -20 \text{ deg}$

G = 200 T/m

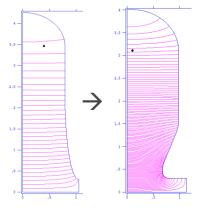
 $L_a = 10.0 \text{ cm}$

Elliptical disk tips



Geometry may be optimized to maximize power efficiency with reasonable peak fields

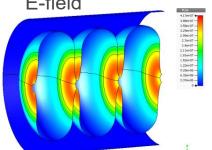
CCL



lattice

Doublet focusing

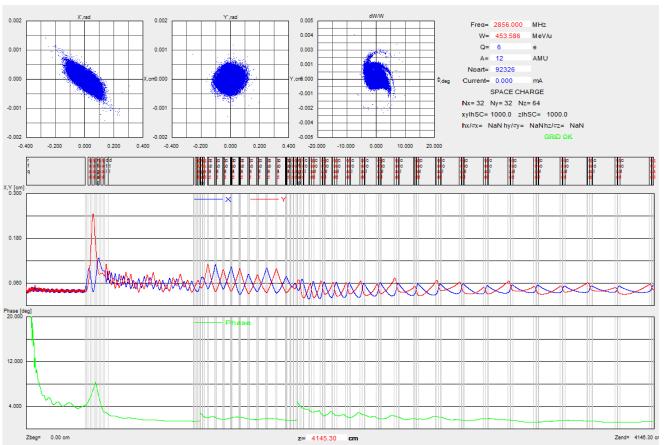
E-field



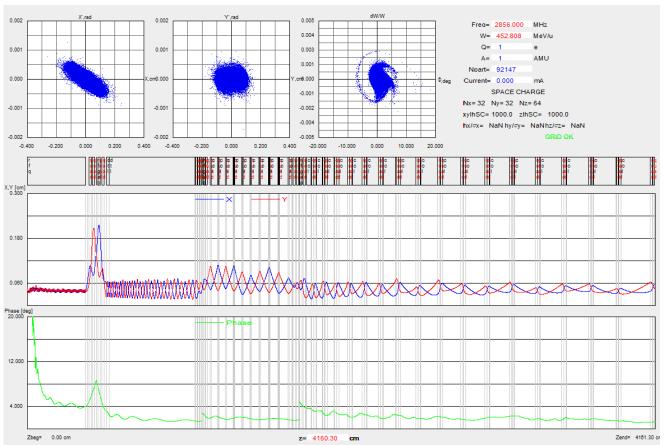
Cells for $\beta = 0.43$

Geometry	Elliptical tips	Drift tubes
Esmax [Kp]	1.9	3.2
ZT² [MΩ/m]	32	59

End-to-end Beam Dynamics - Carbon



End-to-end Beam Dynamics - Protons

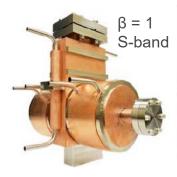


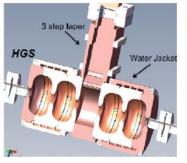






HGS for electrons – built by Radiabeam, tested at Argonne



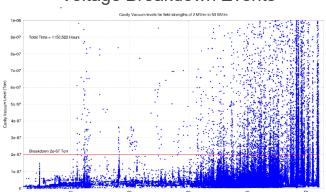


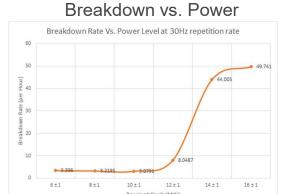
Parameter	Simulated value	
f_{π}	2.856 GHz	
R _s (Effective R _s)	93 MΩ/m (51 MΩ/m)	
Δf	2.5 MHz	
Q_0	19,500	
R/Q	143.2 Ω	
Eacc	50 mV/m	
E _{max} /E _{acc}	1.8	
P _{diss} /cell	2.4 MW	

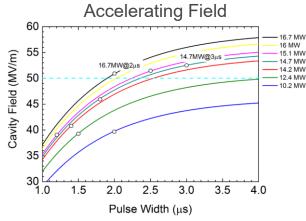


✓ Tested at Argonne's High-Power RF Test Facility (APS) up to 52 MV/m @ 30 Hz

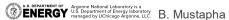








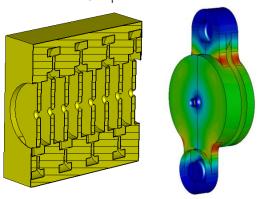
A Structure with similar performance is needed for low-velocity ions ...



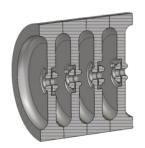
S-Band High-Gradient Structures - Candidates

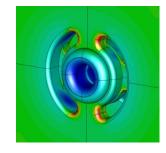
Standing Wave Structures

Side-Coupled Structure

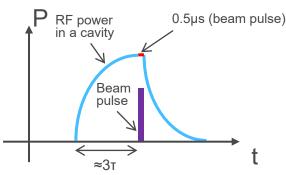


Cut-Disk Structure





SW vs. TW

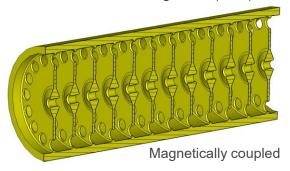


- ✓ SW slow filling, longer pulse than
 TW, affects rep. rate and duty cycle
- ✓ TW requires higher input power to maintain field level and a load to dump output power (~ 50% input)
- ✓ Both have similar power efficiency, peak surface fields and voltage break-down can be minimized
- ✓ SW operate in π-mode, TW offer different phases & harmonics

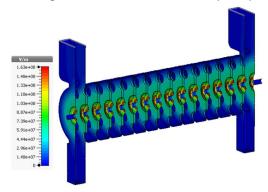
Developments towards ACCIL for Cancer Therapy

Traveling Wave Structures

Backward Traveling Wave $(5\pi/6)$

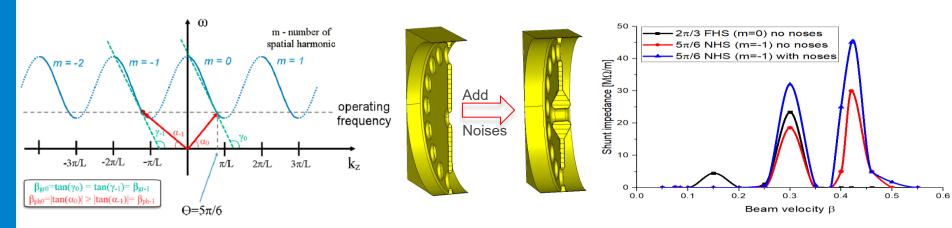


Negative Harmonic Structure $(7\pi/6)$



TW – Space Harmonics – Negative Harmonic

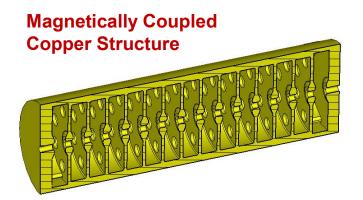
- ✓ In TW, the waveform is not a pure sine but consists of an infinite number of spatial harmonics with the same frequency and group velocity, but with different amplitudes and phase velocities.
- ✓ The phase velocity of higher harmonics is lower, and the period length scales as $L = \beta \lambda |\frac{\theta}{2\pi} + m|$
- ✓ Using the 1st Negative Harmonic, the cell length for $\beta = 0.3$ would be equal to that of $\beta = 0.42$ of the main harmonic \rightarrow enhances power efficiency and allows lower transition energy to HGS for ACCIL



S.V. Kutsaev et al., Phys. Rev. Accel. Beams 20, 120401, 2017.

A Novel High-Gradient Traveling Wave Structure

by Radiabeam (DOE/SBIR), S. Kutsaev et al, Phys. Rev. AB 20 (2017)



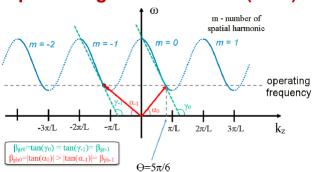
Single Cell Models



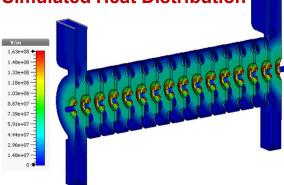
Full Cavity being Tested



Spatial Negative Harmonic (NHS)

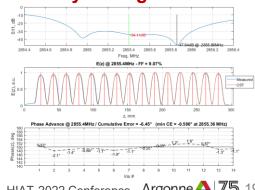


Simulated Heat Distribution



Developments towards ACCIL for Cancer Therapy

Cavity Tuning Results

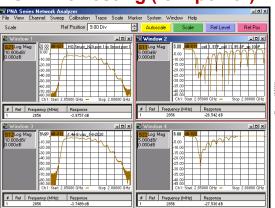


HIAT-2022 Conference

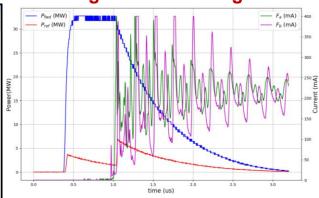
High-Power Testing of the NHS Structure @ ANL



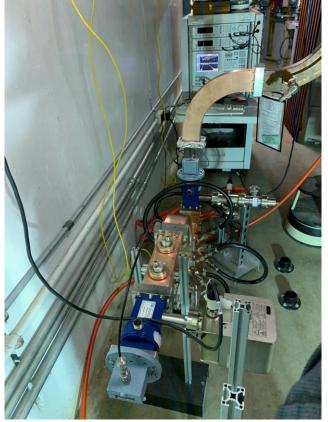
Off-line Testing (low-power)



High-Power Testing



Developments towards ACCIL for Cancer Therapy

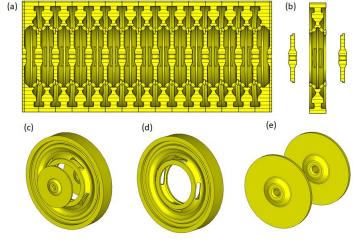


S.V. Kutsaev et al., IEEE Trans. Microw. Wirel. Comp. Lett., 2021

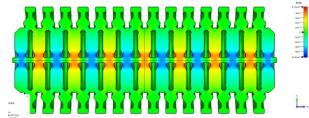
Annular-Coupled HG Standing-Wave Structure

by Argonne (ANL/LDRD), B. Mustapha et al, NAPAC 2019

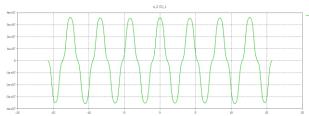
3D Copper Model & Fabrication Method



3D Electric Field Distribution



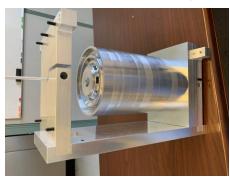
Accelerating Field Profile



Aluminum Model Parts



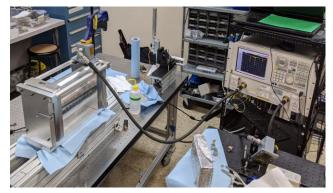
Aluminum Assembly



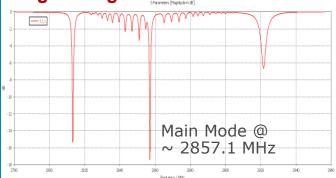
The Aluminum model is being tested to finalize the design and build the actual copper cavity ...

Cold Model Testing of the ACS Structure @ Radiabeam

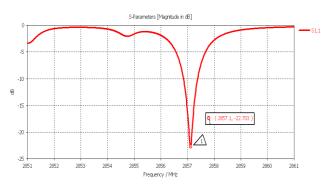
Spectral measurement setup



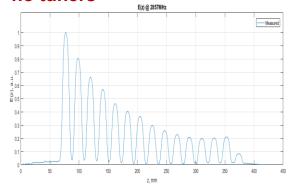
Frequency spectrum, neighboring modes

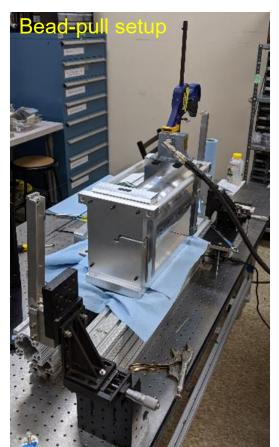


Main mode excitation ~ 2856 MHz



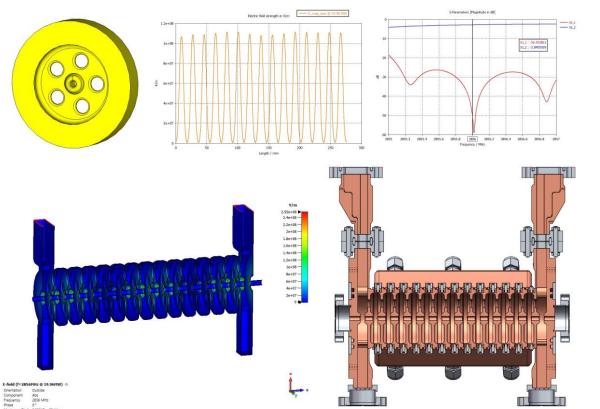
Main mode field profile, no tuners





New NHS for β =0.3 and 1000 Hz rep. rate by Radiabeam

■ 15 cell structure design, tuned including input and output couplers



Repetition rate, Hz	120	1000
Phase velocity, c	0.3	0.3
f, MHz	2856	2856
Repetition rate, Hz	120	1000
Pulse Length, ns	700	587
Input RF Power, MW	33.8	19.9
β _{gr} 1st cell, %c	0.12- 0.335	0.232- 0.43
Fill time, ns	450	287
Shunt Impedance, MΩ/m	32	47
Gradient, MV/m	50	40
Peak E-field @ 40MV/m, MV/m	160	180
Pulse Heating at 1us at 40MV/m, K	28	12.2
<sc>, MW/mm²</sc>	1.3	1.1







ACCIL General Capabilities

- ✓ Capable of accelerating a variety of ion species, proton to neon, up to an energy of 450 MeV per nucleon
- ✓ Pulse-to-pulse energy modulation
- ✓ Intensity modulation at the source or by changing the pulse rep. rate
- ✓ Fast ion beam switching possible from different ion sources in the front-end
- Fast and effective variable energy intensity-modulated multi-ion beam therapy is possible with ACCIL
- ➤ In addition to particle therapy, radiobiology research, imaging R&D and other applications are possible

FLASH Capabilities of the ACCIL Linac

- ✓ FLASH Therapy is a "new" fast dose delivery technique that seems to better spare healthy tissues than the traditional slow and fractionated delivery methods ...
- ✓ FLASH dose requirements: 40 Gy/s to 100 Gy/s
- ✓ For protons at max energy of 230 MeV
 - Beam spot size of $\sim 5x5 \text{ mm}^2$, the beam stopping volume (last 10 cm) is 2.5 cm³
 - Assuming beam looses ½ of its energy, the dose in the stopping volume is 64 Gy/s
 - Need to increase beam size for 40 Gy/s, and 50% more beam for 100 Gy/s
- ✓ For carbon ions at max energy of 450 MeV/u
 - The dose in the stopping volume is 152 Gy/s
 - Need to increase beam size for both 40 Gy/s and 100 Gy/s
- ✓ For all energies and tumor sizes, we would need 10 times more particles per second (10¹¹ protons/s and 10¹⁰ carbon/s), which is still feasible with the ACCIL linac design







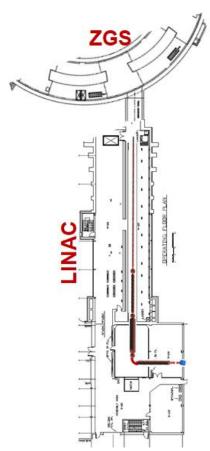
AITRC: An Advanced Ion Therapy Research Center

- √ Cancer therapy and radiobiology research with all ion beams up to neon
- ✓ Imaging / Tomography (ions lighter than carbon: proton, helium, ...)
- ✓ ACCIL Combined with a compact SC gantry, will allow the development of 3D scanning and multi-painting techniques for ions
- ✓ Combined real-time MRI imaging with beam delivery (gantry or straight lines) will significantly enhance the outcome of ion therapy
- ✓ PET imaging using positron emitters (C-11, N-13, O-15, ...) produced in the tumor also possible for dose verification
- ✓ FLASH Therapy and Other Applications ...

Possible Installation at the former IPNS Site

Developments towards ACCIL for Cancer Therapy

- ☐ The former IPNS site is a prime development location for the ACCIL linac and the AITRC center
- ☐ The old Linac building exists and could fit the 50 m ACCIL linac. The AGS building can host several beam lines.
- ☐ The building has the required infrastructure: Water, Power, Cranes ...
- ☐ Using the Linac building and part of ZGS for research & treatment would be a significant cost saving
- ☐ After accelerator development, initial research program: cellular radiobiology & animal prior to human therapy



Thanks to

- ☐ From Argonne
 - A. Nassiri, Y. Yang, D. Meyer and T. Smith
 - A. Barcikowski and R. Fischer
- □ From Radiabeam
 - S. Kutsaev, A. Smirnov, A, Araujo and R. Agustsson
- ☐ From MSU FRIB (contribution while at Argonne)
 - o P. Ostroumov and A. Plastun

- Others



